

(57) Abstract: The invention is directed towards improved structures for use with micro-machined ultrasonic transducers (MUTs), and methods for fabricating the improved structures. In one embodiment, a MUT on a substrate includes an acoustic cavity formed within the substrate at a location below the MUT. The cavity is filled with an acoustic attenuation material to absorb acoustic waves in the substrate, and to reduce parasitic capacitance. In another embodiment, the cavity is formed below a plurality of MUTs, and filled with an attenuation material. In still another embodiment, an attenuation material substantially encapsulates a plurality of MUTs on a dielectric layer. In yet other embodiments, at least one monolithic semiconductor circuit is formed in the substrate that may be operatively coupled to the MUTs to perform signal processing and/or control operations.

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For two-letter codes and other abbreviations, refer to the "Guidance Notes on Codes and Abbreviations" appearing at the beginning of each regular issue of the PCT Gazette.

Micromachined ultrasound transducer and method for fabricating same

TECHNICAL FIELD

This invention relates generally to ultrasound diagnostic systems that use ultrasonic transducers to provide diagnostic information concerning the interior of the body through ultrasound imaging, and more particularly, to micro-machined ultrasonic transducers used in such systems.

BACKGROUND OF THE INVENTION

Ultrasonic diagnostic imaging systems are in widespread use for performing ultrasonic imaging and measurements. For example, cardiologists, radiologists, and obstetricians use ultrasonic diagnostic imaging systems to examine the heart, various abdominal organs, or a developing fetus, respectively. In general, imaging information is obtained by these systems by placing an ultrasonic probe against the skin of a patient, and actuating an ultrasonic transducer located within the probe to transmit ultrasonic energy through the skin and into the body of the patient. In response to the transmission of ultrasonic energy into the body, ultrasonic echoes emanate from the interior structure of the body. The returning acoustic echoes are converted into electrical signals by the transducer in the probe, which are transferred to the diagnostic system by a cable coupling the diagnostic system to the probe.

Acoustic transducers commonly used in ultrasonic diagnostic probes are comprised of an array of individual piezoelectric elements formed from a piezoelectric material by the application of a number of meticulous manufacturing steps. In one common method, a piezoelectric transducer array is formed by bonding a single block of piezoelectric material to a backing member that provides acoustic attenuation. The single block is then laterally subdivided by cutting or dicing the material to form the rectangular elements of the array. Electrical contact pads are formed on the individual elements using various metallization processes to permit electrical conductors to be coupled to the individual elements of the array. The electrical conductors are then coupled to the contact pads by a variety of electrical joining methods, including soldering, spot-welding, or by adhesively bonding the conductor to the contact pad.

Although the foregoing method is generally adequate to form acoustic transducer arrays having up to a few hundred elements, larger arrays of transducer elements having smaller element sizes are not easily formed using this method. Consequently, various techniques used in the fabrication of silicon microelectronic devices have been adapted to form ultrasonic transducer elements, since these techniques generally permit the repetitive fabrication of small structures in intricate detail.

An example of a device that may be formed using semiconductor fabrication methods is the micro-machined ultrasonic transducer (MUT). The MUT has several significant advantages over conventional piezoelectric ultrasonic transducers. For example, the structure of the MUT generally offers more flexibility in terms of optimization parameters than is typically available in conventional piezoelectric devices. Further, the MUT may be conveniently formed on a semiconductor substrate using various semiconductor fabrication methods, which advantageously permits the formation of relatively large numbers of transducers, which may then be integrated into large transducer arrays. Additionally, interconnections between the MUTs in the array and electronic devices external to the array may also be conveniently formed during the fabrication process. MUTs may be operated capacitively, and are referred to as cMUTs, as shown in U.S. Patent No. 5,894,452. Alternatively, piezoelectric materials may be used to fabricate the MUT, which are commonly referred to as pMUTs, as shown in U.S. Patent No. 6,049,158. Accordingly, the MUT has increasingly become an attractive alternative to conventional piezoelectric ultrasonic transducers in ultrasound systems.

Figure 1 is a partial cross sectional view of a MUT 1 according to the prior art. The MUT 1 may have a planform that is rectangular, circular, or may be of other regular shapes. The MUT 1 generally includes an upper surface 2 that is spaced apart from a lower surface 3 that abuts a silicon substrate 5. Alternatively, a dielectric layer 4 may be formed on the substrate 5 that underlies the MUT 1. When a time-varying excitation voltage (not shown) is applied to the MUT 1, a vibrational deflection in the upper surface 2 is developed that stems from the electro-mechanical properties of the MUT 1. Accordingly, acoustic waves 6 are created that radiate outwardly from the upper surface 2 in response to the applied time-varying voltage. The electro-mechanical properties of the MUT 1 similarly allow the MUT 1 to be responsive to deflections resulting from acoustic waves 7 that impinge on the upper surface 2.

One disadvantage in the foregoing prior art device is that a portion of the ultrasonic energy developed by the MUT 1 may be projected backwardly into the underlying

substrate 5, rather than being radiated outwardly in the acoustic wave 6, which results in a partial loss of radiated energy from the MUT 1. Moreover, when ultrasonic energy is coupled into the underlying substrate 5, various undesirable effects are produced, which are briefly described below.

5 With reference now to Figure 2, a partial cross sectional view of a MUT array 10 according to the prior art is shown. The array 10 includes a plurality of MUT transducers 1 formed on a silicon substrate 5. Each transducer 1 is coupled to a time-varying voltage source through a plurality of electrical interconnections formed in the substrate 5. For clarity of illustration, the voltage source and the electrical interconnections are not shown. An
10 acoustic wave 21 may be conducted into the substrate 5 through a back surface 3. The wave 21 propagates within the substrate 5 and is internally reflected at a lower surface 18 of the substrate 5 to form a reflected wave 23 that is directed towards an upper surface 19 of the substrate 5. Consequently, a plurality of reflected waves 23 propagate within the substrate 5 between the upper surface 19 and the lower surface 18. A portion of the energy present in
15 each reflected wave 23 may also leave the substrate 5 through the surface 18, to form a plurality of leakage waves 25. An internal reflection 27 from an end 24 of the array 10 may lead to still further reflected waves 27 and leakage waves 26.

 The propagation of acoustic waves 23 and 27 in the substrate 5, as described above, permits ultrasonic energy to be cross-coupled between the plurality of MUT
20 transducers 1 on the substrate 5 and produce undesirable "cross-talk" signals between the plurality of MUTs 1, as well as other undesirable interference effects. Still further, the internal reflection of waves in the substrate 5 may adversely affect the acceptance angle, or directivity of the array 10.

 Various prior art devices have included elements that impede the propagation
25 of waves in the substrate. For example, one prior art device employs a plurality of trenches between the MUTs 1 that extend downwardly into the substrate 5 to interrupt wave propagation within the substrate 5. Another prior art device employs a similar downwardly projecting trench, and fills the trench with an acoustic absorbing material in order to at least partially absorb the energy in the reflected waves 23. Other prior art devices minimize lateral
30 wave propagation by controlling still other geometrical details of the array. Although these prior art devices generally reduce the undesired lateral wave propagation in the substrate, they generally limit the design flexibility inherent in the MUT by reducing the number of design parameters that may be independently varied. Furthermore, the additional manufacturing steps significantly increase the manufacturing cost of arrays that use MUTs.

A further disadvantage associated with the prior art devices shown in Figures 1 and 2 is that a relatively large parasitic capacitance may be formed between the one or more MUTs 1 and the underlying substrate 5. Since the MUT 1 is an electro-mechanical device that is generally excited by frequencies in the megahertz range, the formation of parasitic capacitances between the MUTs 1 and the substrate 5 further degrade the performance of the MUTs 1 by producing an additional capacitive load that generally degrades the sensitivity of the MUT.

Accordingly, there is a need in the art for micro-machined ultrasonic transducer structures that are capable of producing significant reductions in acoustic wave propagation in the underlying substrate. Further, there is a need in the art for a micro-machined ultrasonic transducer structures that suppress parasitic capacitive coupling between a MUT and an underlying substrate.

SUMMARY OF THE INVENTION

The invention is directed towards improved structures for use with micro-machined ultrasonic transducers (MUTs), and methods for fabricating the improved structures. In one aspect, a MUT is formed on a substrate and an acoustic cavity is formed within the substrate at a location below the MUT. The acoustic cavity is filled with an acoustic attenuation material to absorb acoustic waves propagated into the substrate, and to reduce the effect of parasitic capacitances on the operation of the MUT. In another aspect, the acoustic cavity is formed below a plurality of MUTs that comprise an array. The acoustic cavity and the acoustic attenuation material substantially reduce cross coupling between the MUTs by preventing wave propagation in the substrate. In still another aspect, a plurality of MUTs about a dielectric layer with the MUTs being substantially encapsulated by the acoustic attenuation material. In yet another aspect, at least one monolithic semiconductor circuit is formed in the substrate that may be operatively coupled to the MUTs, the circuit being positioned in a non-etched portion of the substrate. In still another aspect, the at least one monolithic semiconductor circuit is formed in the substrate and positioned in a thin substrate layer above the acoustic cavity. In yet another aspect, a plurality of MUTs is attached to one side of a layer of semiconductor material, and a dielectric layer is formed on the opposing side. At least one monolithic semiconductor circuit is formed in the semiconductor material that may be operatively coupled to the MUTs.

BRIEF DESCRIPTION OF THE DRAWINGS

Figure 1 is a partial cross sectional view of a MUT transducer according to the prior art.

5 Figure 2 is a partial cross sectional view of a MUT transducer array according to the prior art.

Figure 3 is a partial cross sectional view of a MUT transducer assembly according to an embodiment of the invention.

Figure 4 is a partial cross sectional view of a MUT transducer array according another embodiment of the invention.

10 Figure 5 is a partial cross sectional view of a MUT transducer illustrating a step in a method of fabricating the MUT transducer according to still another embodiment of the invention.

Figure 6 is a partial cross sectional view of a MUT transducer illustrating a step in a method of fabricating the MUT transducer according to still another embodiment of the invention.

15 Figure 7 is a partial cross sectional view of a MUT transducer illustrating a step in a method of fabricating the MUT transducer according to still another embodiment of the invention.

Figure 8 is a partial cross sectional view of a MUT transducer illustrating a step in a method of fabricating the MUT transducer according to still another embodiment of the invention.

Figure 9 is a partial cross sectional view of a MUT transducer array according still another embodiment of the invention.

20 Figure 10 is a partial cross sectional view of a MUT transducer illustrating a step in a method of fabricating the MUT transducer according to still yet another embodiment of the invention.

Figure 11 is a partial cross sectional view of a MUT transducer illustrating a step in a method of fabricating the MUT transducer according to still yet another embodiment of the invention.

30 Figure 12 is a partial cross sectional view of a MUT transducer illustrating a step in a method of fabricating the MUT transducer according to still yet another embodiment of the invention.

Figure 13 is a partial cross sectional view of a MUT transducer array according another embodiment of the invention.

Figure 14 is a partial cross sectional view of a MUT transducer array according yet another embodiment of the invention.

Figure 15 is a partial cross sectional view of a MUT transducer array according still another embodiment of the invention.

5 Figure 16 is a partial cross sectional view of a MUT transducer array according to yet still another embodiment of the invention.

DETAILED DESCRIPTION OF THE INVENTION

The present invention is generally directed to ultrasound diagnostic systems that use micro-machined ultrasonic transducers (MUTs) to provide diagnostic information concerning the interior of the body through ultrasound imaging. Many of the specific details of certain embodiments of the invention are set forth in the following description and in Figures 3 through 16 to provide a thorough understanding of such embodiments. One skilled in the art will understand, however, that the present invention may be practiced without several of the details described in the following description. Further, it is understood that the MUT described in the embodiments below may include any electro-mechanical device that may be formed on a semiconductor substrate that is capable of emitting acoustic waves when excited by a time-varying voltage, and producing a time-varying electrical signal when stimulated by acoustic waves. Accordingly, the MUT may include a capacitive micro-machined ultrasonic transducer (cMUT), a piezoelectric micro-machined ultrasonic transducer (pMUT), or still other micro-machined ultrasonic devices. Moreover, in the description that follows, it is understood that the figures related to the various embodiments are not to be interpreted as conveying any specific or relative physical dimension, and that specific or relative dimensions related to the various embodiments, if stated, are not to be considered limiting unless the claims expressly state otherwise.

Figure 3 is a partial cross sectional view of a MUT transducer array 30 according to an embodiment of the invention. The MUT transducer array 30 includes a MUT 32 formed on a substrate 34. The array 30 is capable of receiving ultrasonic waves and generating an output electrical signal, and generating ultrasonic waves in response to input electrical signals. The input and output signals are exchanged with an ultrasound system (not shown) through a plurality of interconnections positioned within the substrate 34. For clarity of illustration, the interconnecting portions are not shown in Figure 3. The MUT 32 may be formed on the substrate 34 through the application of a series of well-known semiconductor fabrication processes. For example, the MUT 32 may be formed by patterning a surface of

the substrate using a photolithographic process, and successively adding material layers to the substrate 34 by various material deposition processes. Structural features of the MUT 32 may further be formed by removing selected portions of the deposited material through the application of various etching processes. A dielectric layer may optionally be formed on an upper substrate surface 35 that electrically isolates the MUT 32 from the underlying substrate 34. Alternatively, the dielectric layer may be incorporated directly into the MUT 32.

Still referring to Figure 3, the array 30 further includes a cavity 36 that is formed within the substrate 34. The cavity 36 extends from an upper cavity surface 37 and proceeds downwardly towards a lower substrate surface 39. The cavity 36 also includes a pair of sidewalls 38 that depend downwardly from the upper cavity surface 37 to the lower substrate surface 39. The upper cavity surface 37 is separated from the upper surface 35 by a separation layer 31 that is sufficiently thin to prevent the significant propagation of acoustic waves to other portions of the substrate 34. The cavity 36 may be filled with an acoustic attenuation material 33 having a relatively high acoustic attenuation to provide an acoustically-damped region below the MUT 32. The dimensions of the cavity 36 and the characteristics of the material 33 cooperatively yield an acoustic impedance that is compatible with the overall acoustic design of the array 30. For example, the depth "d" of the cavity 36 may be sufficient to allow waves transmitted from the MUT 32 through the surface 35 to be attenuated to a relatively negligible level, since the material 33 is sufficiently lossy to dissipate the acoustic energy present in the waves. Accordingly, the material 33 may include an elastomeric material, such as a room temperature vulcanizing (RTV) elastomer, or various epoxy matrices having dispersed solid metallic, ceramic, or polymeric filler particles of a selected density. Still further, the epoxy matrix may be filled with elastomeric particles or air-filled "micro-balloons" to achieve the desired acoustic properties. The array 30 may be positioned on an acoustic backing member (not shown) to support the array 30 and to provide further acoustic attenuation.

Figure 4 is a partial cross sectional view of a MUT transducer array 40 according to another embodiment of the invention. The MUT transducer array 40 includes a plurality of MUTs 32 formed on a substrate 34 in a predetermined pattern to form the array 40. A cavity 36 is formed below the plurality of MUTs 32 that extends downwardly from an upper cavity surface 37 towards a lower substrate surface 39. The cavity 36 is dimensioned to yield a predetermined acoustic impedance when the cavity 36 is filled with a selected acoustic material 33.

Figures 5 through 8 are partial cross sectional views that illustrate the steps in a method for fabricating a MUT array according to another embodiment of the invention. Referring to Figure 5, a MUT 32 is formed on a substrate 34 by a sequence of well-known semiconductor fabrication steps, which may include the formation of a dielectric layer 50 on an upper surface 51 of the substrate 34. The dielectric layer 50 may include silicon dioxide or silicon nitride, although other dielectric materials including silicon oxynitrides may be used. A layer 53 of silicon dioxide or silicon nitride is deposited on a lower surface 52. The layer 53 is patterned using standard photolithographic processes to create an opening in the layer 53, providing access to the back surface 52 of the substrate 34.

Turning now to Figure 6, the substrate 34 may then be etched to form a cavity 36 that extends from the lower surface 52 to an upper cavity surface 37, as shown in Figure 7. The dielectric layer 50 may also serve as an etch stop layer during the etching process, although other etch stop devices, such as selective doping of the substrate 34, may also be used. The substrate 34 may be etched using a variety of isotropic or anisotropic solutions in an etching bath to form the cavity 36. The material properties of the substrate 34 and the composition of the etching bath generally cooperatively determine the shape of the cavity 36. For example, if the substrate 34 is monocrystalline silicon having a $\langle 111 \rangle$ crystalline orientation, then an etching solution comprised of hydrofluoric acid and nitric acid will form a cavity 36 having side walls 38 that extend inwardly at approximately 45 degrees. Alternatively, a $\langle 100 \rangle$ monocrystalline material etched with a potassium hydroxide etching solution will yield side walls that extend inwardly at approximately 54.7 degrees. Other internal shapes for the cavity 36 may be obtained using other crystalline configurations in the substrate 34 together with other etching solutions, and are considered to be within the scope of the invention. Similarly, methods other than wet etching may be used to form the cavity 36. For example, dry etching methods, which include plasma etching, ion beam milling and reactive ion etching may be also used.

Referring now to Figure 8, the cavity 36 may be filled with an acoustic material 33, which may be comprised of any of the materials identified above. The material 33 may be deposited into the acoustic cavity 36 by direct injection of the material 33 into the cavity 36, although other methods exist. For example, the material 33 may be sprayed into the cavity 36. Following the application of the material 33, the layer 53 may be stripped to expose the surface 52. The layer 53 may be stripped using various stripping methods, including wet chemical stripping or plasma stripping methods. An acoustic backing member may be positioned below the array to provide further acoustic attenuation.

The foregoing embodiments advantageously provide an acoustic cavity below the one or more MUT devices that is filled with an acoustic material to substantially inhibit the propagation of acoustic waves in the substrate. Additionally, the attenuation material generally possesses an acoustic impedance that substantially differs from the substrate material, permitting the MUT to transmit and receive ultrasonic signals more effectively. Still further, by positioning the substantially non-electrically conductive attenuation material below the one or more MUTs, parasitic capacitive coupling effects that may adversely affect the performance of the MUTs are reduced.

Figure 9 is a partial cross sectional view of a MUT transducer array 60 according still another embodiment of the invention. The array 60 includes a plurality of MUTs 32 that are attached to a dielectric layer 50. The MUTs 32 are further embedded in an acoustic attenuation material 62 that substantially encapsulates the MUTs 32 and abuts the dielectric layer 50 at locations 64. The material 62 further substantially fills spaces 66 between adjacent MUTs 32 to provide additional resistance to cross-coupling effects. The acoustic attenuation material 62 extends a distance "d" below the layer 50 to ensure that waves propagated into the material 62 are substantially attenuated. The acoustic attenuation material 62 may include an elastomeric material, such as a room temperature vulcanizing (RTV) elastomer, or various epoxy matrices having dispersed solid metallic, ceramic, or polymeric filler particles of a selected density. Still further, the epoxy matrix may be filled with elastomeric particles or air-filled "micro-balloons" to achieve the desired acoustic properties.

Still referring to Figure 9, the dielectric layer 50 is a thin structure that permits acoustic waves 6 generated by each of the MUTs 32 in the array 60 to be transmitted outwardly, and correspondingly permits reflected acoustic waves 7 to be received by the MUTs 32. Accordingly, the layer 50 may be comprised of a thin layer of silicon dioxide or silicon nitride, although other alternatives exist.

Figures 10 through 12 are partial cross sectional views that illustrate the steps in a method for fabricating a MUT array according to another embodiment of the invention. Referring to Figure 10, a dielectric layer 50 is formed on a substrate 34. A plurality of MUTs 32 are similarly formed on the substrate 34, with the dielectric layer 50 interposed between the MUTs 32 and the substrate 34. Alternatively, the substrate 34 may be comprised of a silicon-on-insulator (SOI) substrate that includes a layer of dielectric material that is spaced apart from the MUTs 32 and positioned within the substrate 32, so that the MUTs 32 are positioned directly on a silicon surface. An acoustic attenuation material 62 is formed over

the plurality of MUTs 32 that substantially encapsulates the MUTs 32, as shown in Figure 11.

Turning to Figure 12, the substrate 34 is substantially removed to expose an upper dielectric surface 64. If the substrate 34 is an SOI substrate, then the substrate 34 is thinned to expose the insulating layer. In either case, the substrate 34 may be removed by wet etching the substrate 34 in a suitable solution, although other alternative methods exist. For example, the substrate 34 may be removed by employing wet spin etching to remove the substrate 34. The dielectric layer 50 may serve as an etch stop layer during the etching process. The substrate 34 may also be removed by backgrinding the substrate 34 to expose the surface 64.

In addition to the advantages previously identified in connection with other embodiments, the foregoing embodiments additionally provide an unbounded acoustic cavity that advantageously permits the entire MUT to be encapsulated, so that spaces between adjacent MUTs are filled with the acoustic attenuation material, thus further reducing cross-coupling effects.

Figure 13 is a partial cross sectional view of a MUT transducer array 70 according another embodiment of the invention. The MUT transducer array 70 includes a plurality of MUTs 32 formed on a substrate 34 in a predetermined pattern. A dielectric layer 50 may be interposed between the plurality of MUTs 32 and the substrate 34 to provide electrical isolation. An attenuation cavity 36 is formed below the plurality of MUTs 32 that extends downwardly from an upper cavity surface 37 towards a lower substrate surface 39. The cavity 36 may be filled with an acoustic attenuation material 33 to yield selected acoustic properties for the array 70. The array 70 further includes at least one semiconductor circuit 72 that is monolithically formed in the substrate 34 that is positioned proximate to a side of the attenuation cavity 36. The circuit 72 may include a single semiconductor device, such as a field effect transistor (FET) or a similar device, which is used to drive the MUTs. Alternatively, the circuit 72 may comprise more fully integrated devices. For example, the circuit 72 may include monolithically formed circuits that at least partially perform receiver functions, beamforming processing, or other "front end" processing for the array 70. Further, the circuit 72 may also include circuits that perform control operations for the array 70. The semiconductor circuit 72 may be interconnected with the plurality of MUTs 32 and to other circuits external to the array by interconnecting elements formed in the substrate (not shown). The MUT transducer array 70 may be positioned on an acoustic backing member (not shown) to support the array 70 and to provide further acoustic attenuation.

Figure 14 is a partial cross sectional view of a MUT transducer array 80 according yet another embodiment of the invention. The MUT transducer array 80 includes a plurality of MUTs 32 formed on a substrate 34, which may have a dielectric layer 50 interposed between the plurality of MUTs 32 and the substrate 34. An attenuation cavity 36 is formed below the plurality of MUTs 32 that extends downwardly from an upper cavity surface 37 towards a lower substrate surface 39. The cavity 36 may be filled with an acoustic attenuation material 33 to yield selected acoustic properties for the array 80. The array 80 further includes at least one semiconductor circuit 82 that is monolithically formed in a separation layer 31 at a location above the attenuation cavity 36, and proximate to the plurality of MUTs 32. As in the previous embodiment, the circuit 82 may include a single semiconductor device, or the circuit 82 may comprise more fully integrated devices. The semiconductor circuit 82 may be interconnected with the plurality of MUTs 32 and to other circuits external to the array by interconnection elements formed in the substrate (not shown). Alternatively, at least one circuit 82 may be formed in the separation layer 31 at a position approximately below the plurality of MUTs 32 and form interconnections (not shown) with the MUTs 32 through vias (also not shown) that extend from the MUTs 32 to the at least one circuit 82. The MUT transducer array 80 may be positioned on an acoustic backing member (not shown) to support the array 80 and to provide still further acoustic attenuation.

Figure 15 is a partial cross sectional view of a MUT transducer array 90 according still another embodiment of the invention. The array 90 includes a plurality of MUTs 32 embedded in an acoustic attenuation material 62 that substantially encapsulates the MUTs 32. A layer 94 comprised of a semiconductor material is interposed between a dielectric layer 96 and the plurality of MUTs 32. The dielectric layer 96 may be comprised of a thin layer of silicon dioxide or silicon nitride, although other alternatives exist. The array 90 further includes at least one semiconductor circuit 92 that is monolithically formed in the layer 94 at a location proximate to the plurality of MUTs 32. As described in detail in connection with other embodiments of the invention, the circuit 92 may include a single device, or may comprise more fully integrated devices, including circuits that at least partially perform receiver, beamforming processing, or still other operations. The semiconductor circuit 92 may be interconnected with the plurality of MUTs 32 and to other circuits external to the array by conductive elements formed in the substrate (not shown). Alternatively, at least one circuit 92 may be formed in the layer 94 at a position approximately below the plurality of MUTs 32 and form interconnections (not shown) with

the MUTs 32 through vias (also not shown) that extend from the MUTs 32 to the at least one circuit 92.

Fabrication of the array 90 of Figure 15 may proceed generally as shown in Figures 10 through 12. A dielectric layer 96 may be formed on a silicon substrate 34 (as shown in Figure 10). Alternatively, a silicon-on-insulator (SOI) substrate may be used to provide both the substrate 34 and the dielectric layer 96. In either case, the semiconductor circuits 92 are formed where desired in the layer 94. The MUTs 32 may then be formed in the layer 94 and a surface of the array 90 that includes the MUTs may be covered with the acoustic attenuation material 62. The substrate 34 may then be removed by backgrinding, etching, or other similar methods to yield the array 90 shown in Figure 15.

Figure 16 is a partial cross sectional view of a MUT transducer array 100 according to yet still another embodiment of the invention. The array 100 is similar to the embodiment shown in Figure 15 with the dielectric layer 96 removed, and at least a portion of the layer 94 removed, or not formed. Since the layer 96 and 94 are removed, acoustic attenuation due to the layers 96 and 94 are largely eliminated, so that the receiving and transmitting abilities of the MUTs 32 is enhanced. In addition, the layer 94 may be left or formed as islands (not shown) that may be used to form additional circuits 92, either adjacent to, or between the MUTs 32.

In addition to the advantages present in other embodiments of the invention, the foregoing embodiments include at least one semiconductor circuit that is monolithically formed in the substrate, and positioned in the substrate at a location proximate to the MUTs. The semiconductor circuit advantageously permits at least a portion of the signal processing and/or control circuits for the MUTs to be formed on a common substrate, resulting in significant cost savings through reduced hardware requirements, and savings in fabrication costs.

The above description of illustrated embodiments of the invention is not intended to be exhaustive or to limit the invention to the precise form disclosed. While specific embodiments of, and examples of, the invention are described in the foregoing for illustrative purposes, various equivalent modifications are possible within the scope of the invention, as those skilled within the relevant art will recognize. For example, the cavity formed behind the MUTs is, as mentioned above, generally filled with an acoustic material, and the filled cavity or the thinned substrate layer are generally backed with acoustic backing material in the form of a layer or backing block having attenuative and impedance characteristics chosen in accordance with the requirements of the particular application. One

or the other or both the cavity and backing may alternatively be air-filled, which may be desirable in low frequency applications, or when transmitting acoustic waves into air. The cavity and backing material may have strong attenuative (lossy) properties, or reflective or matching characteristics, depending upon the particular application. Still further, the various
5 embodiments described above can be combined to provide further embodiments.
Accordingly, the invention is not limited by the disclosure, but instead the scope of the invention is to be determined entirely by the following claims.

CLAIMS:

1. A micro-machined ultrasonic transducer array, comprising:
a substrate having an upper surface and an opposing lower surface and a thickness there between;
a recess formed in the substrate that projects upwardly into the substrate from
5 the lower surface to an intermediate position within the substrate, the recess being substantially filled with a material having a predetermined acoustic property; and
at least one micro-machined ultrasonic transducer (MUT) supported by the upper surface of the substrate and positioned over the recess.
- 10 2. The array according to claim 1 wherein the MUT is further comprised of a capacitive micro-machined ultrasonic transducer (cMUT) or a piezoelectric micro-machined ultrasonic transducer (pMUT).
3. The array according to claim 1, further comprising a dielectric layer interposed
15 between the substrate and the at least one MUT.
4. The array according to claim 1 wherein the material is further comprised of an elastomeric material.
- 20 5. The array according to claim 1 wherein the material is further comprised of an epoxy resin material.
6. The array according to claim 5 wherein the epoxy resin material is further comprised of an epoxy resin material with a filler material.
25
7. The array according to claim 1, further comprising a backing member that abuts the lower surface.
8. A micro-machined ultrasonic transducer array, comprising:

at least one micro-machined ultrasonic transducer (MUT) formed on a substrate which has been substantially entirely removed; and
an acoustic material of predetermined acoustic properties that substantially encapsulates the at least one MUT.

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9. A method for fabricating a micro-machined ultrasonic transducer array, comprising:
forming at least one micro-machined ultrasonic transducer (MUT) on a surface of a substrate;
10 removing a portion of the substrate to form a recess that underlies the at least one MUT; and
disposing an acoustic attenuation material into the recess.

10. A method for fabricating a micro-machined ultrasonic array, comprising:
15 forming at least one micro-machined ultrasonic transducer (MUT) on a substrate material;
depositing an acoustic attenuation material on the substrate that substantially encapsulates the at least one MUT; and
removing at least a substantial portion of the substrate material from the
20 acoustic attenuation material and MUT.

1/7

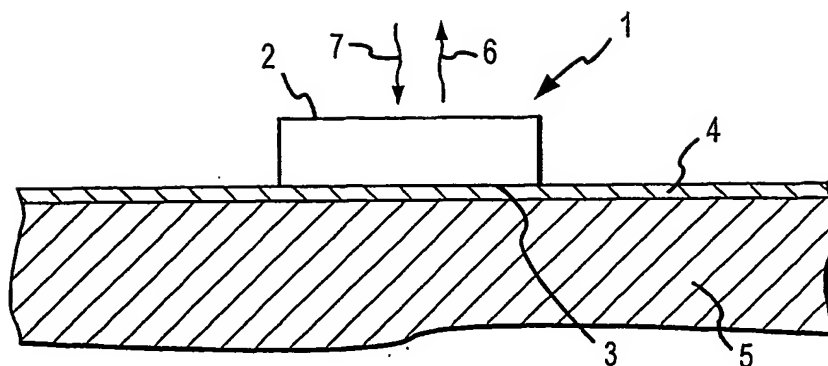


FIG. 1
(PRIOR ART)

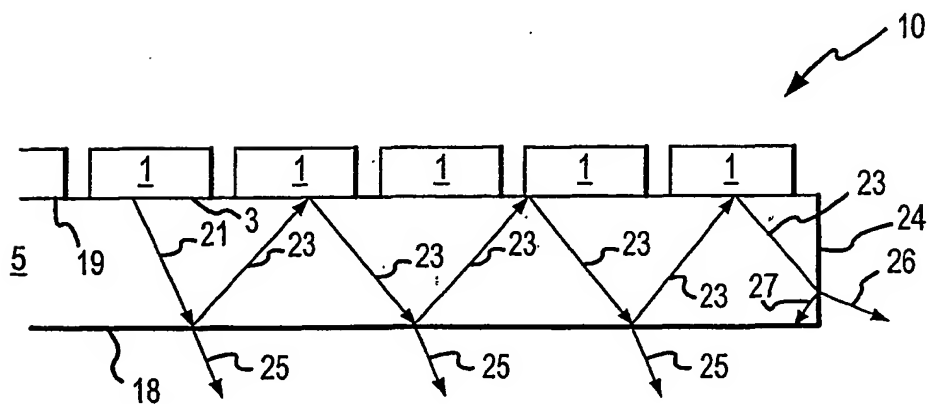


FIG. 2
(PRIOR ART)

2/7

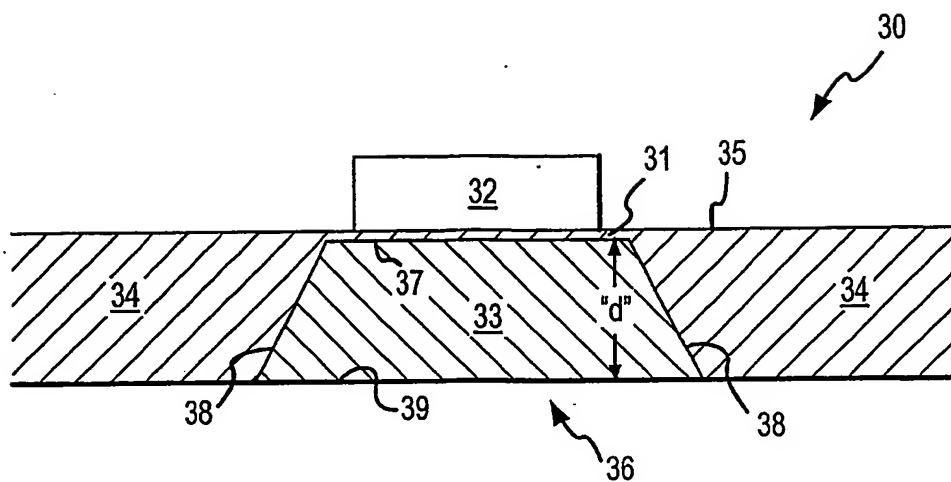


FIG. 3

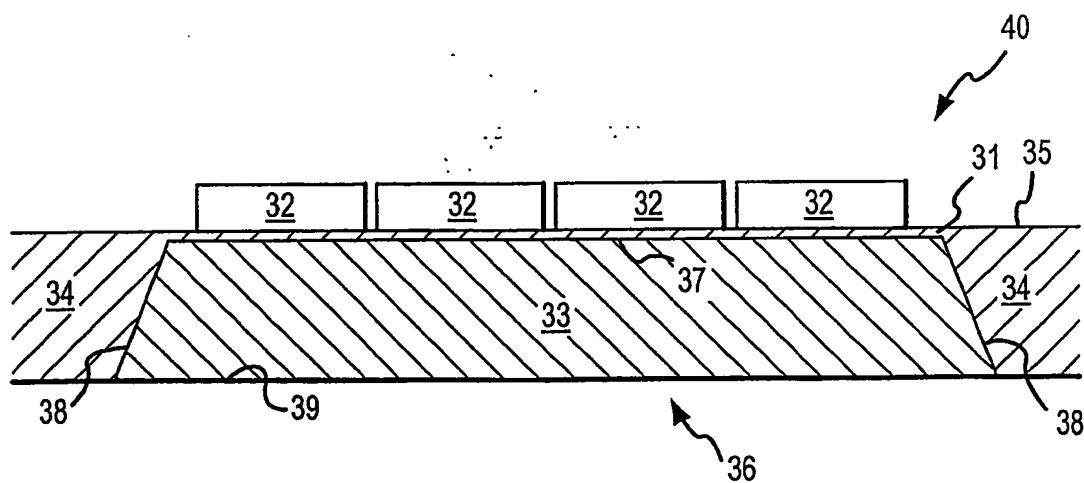


FIG. 4

3/7

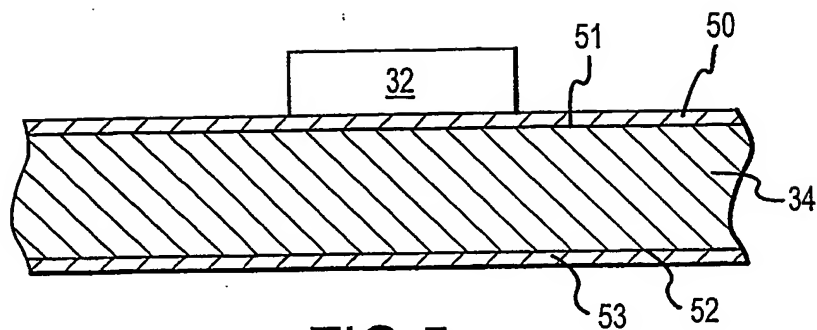


FIG. 5

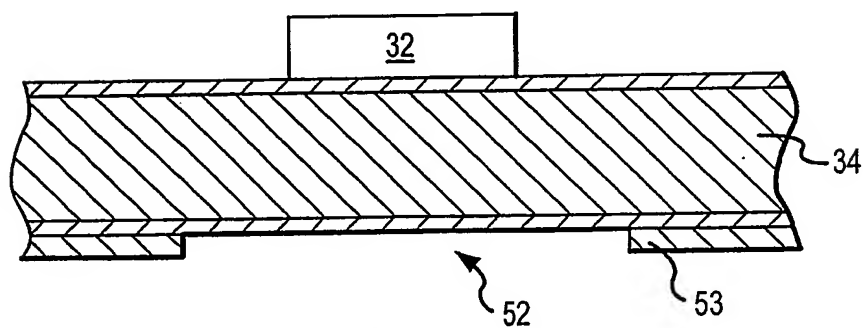


FIG. 6

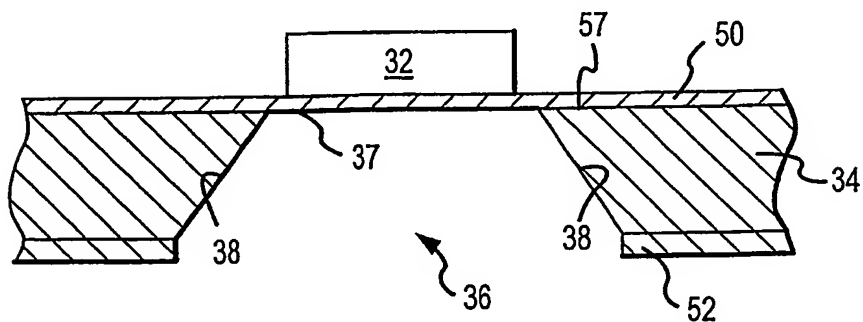


FIG. 7

4/7

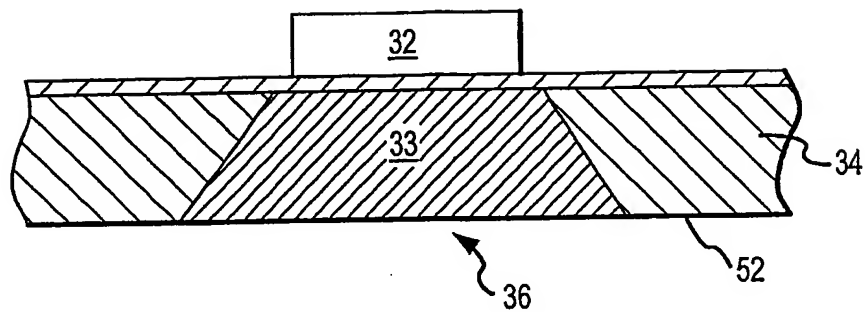


FIG.8

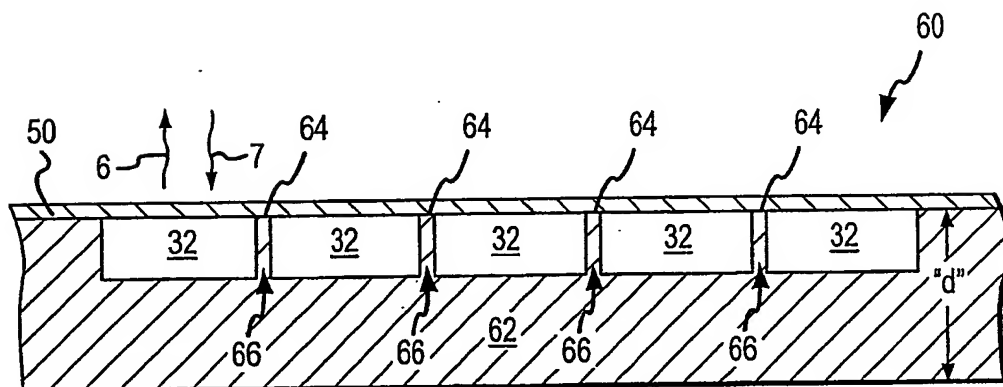


FIG.9

5/7

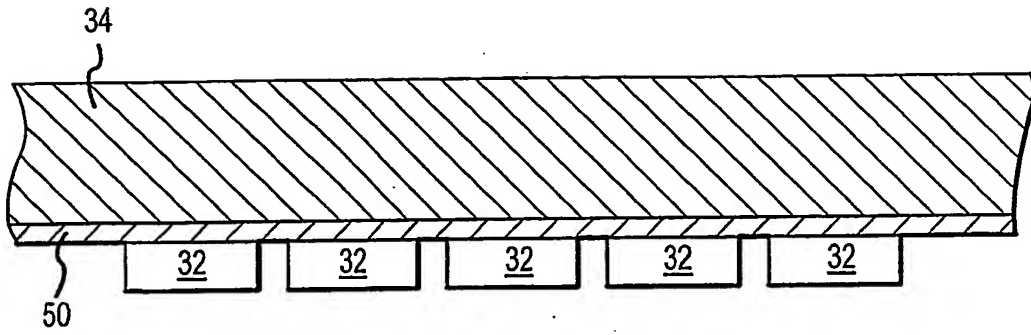


FIG. 10

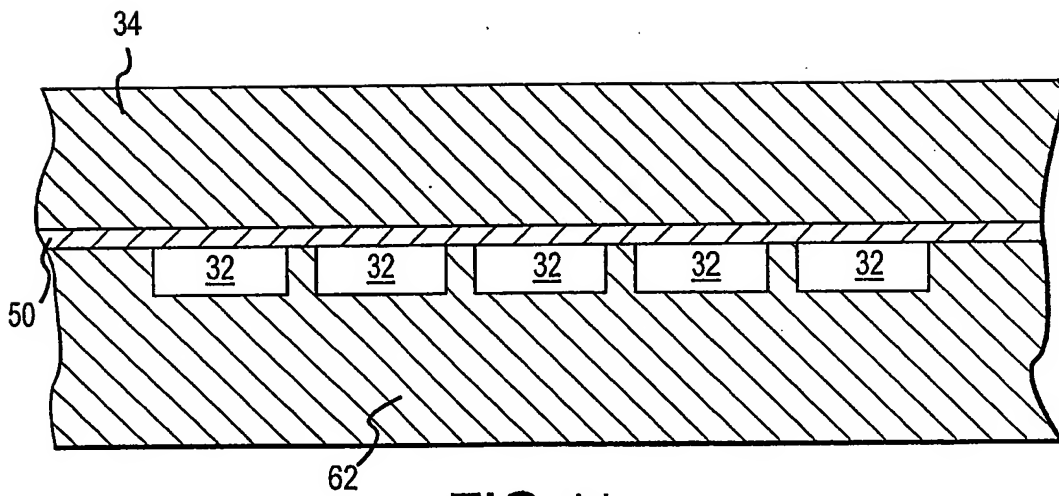


FIG. 11

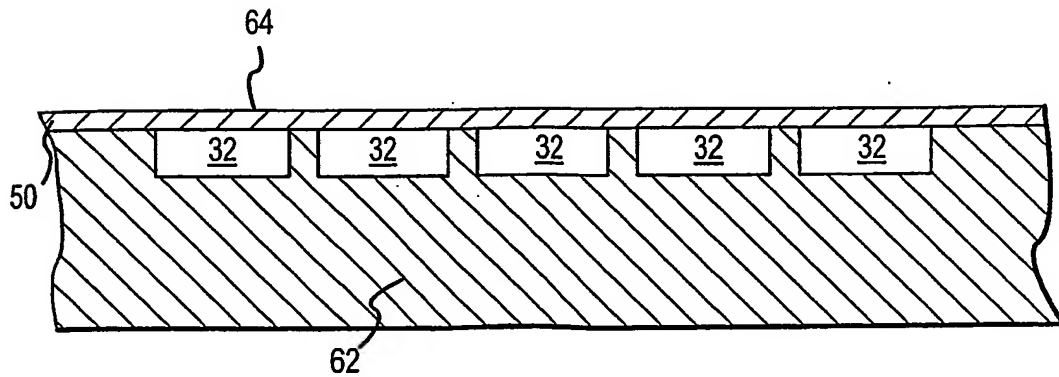


FIG. 12

6/7

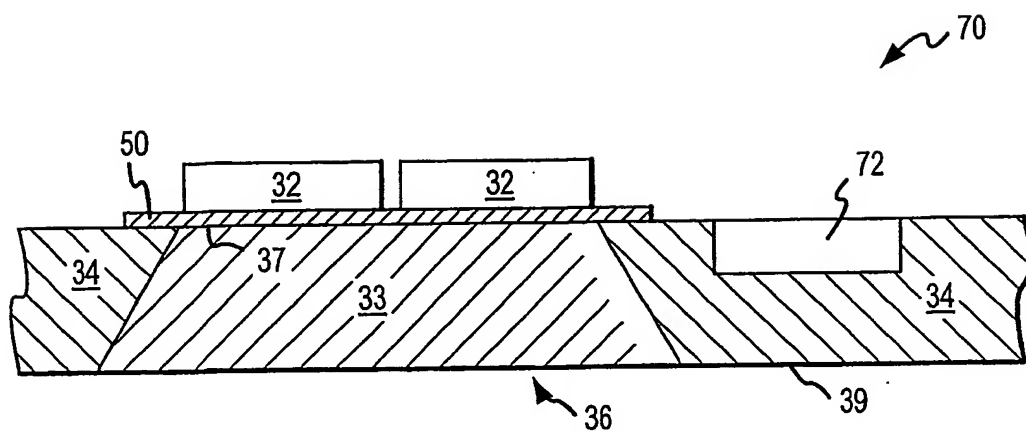


FIG. 13

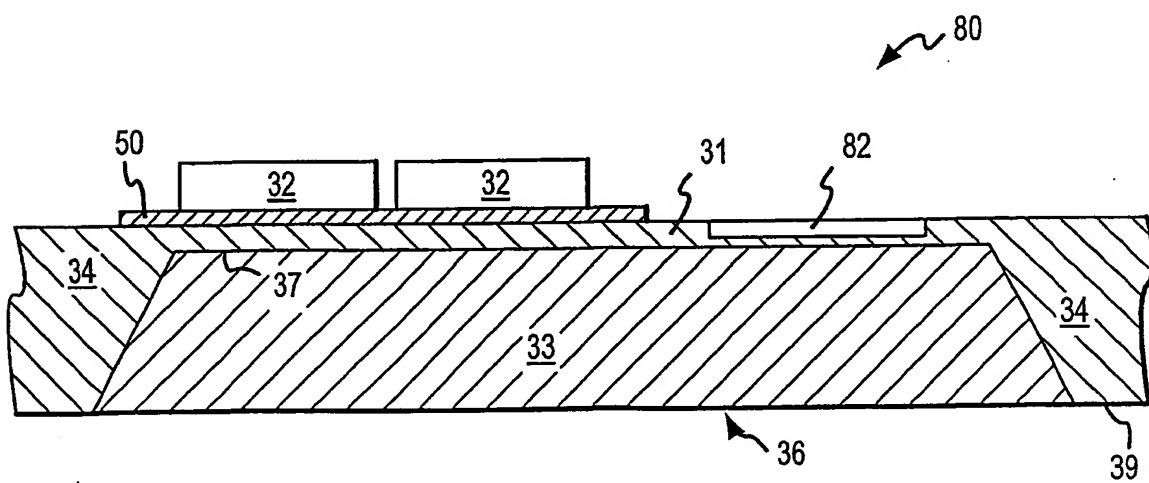


FIG. 14

7/7

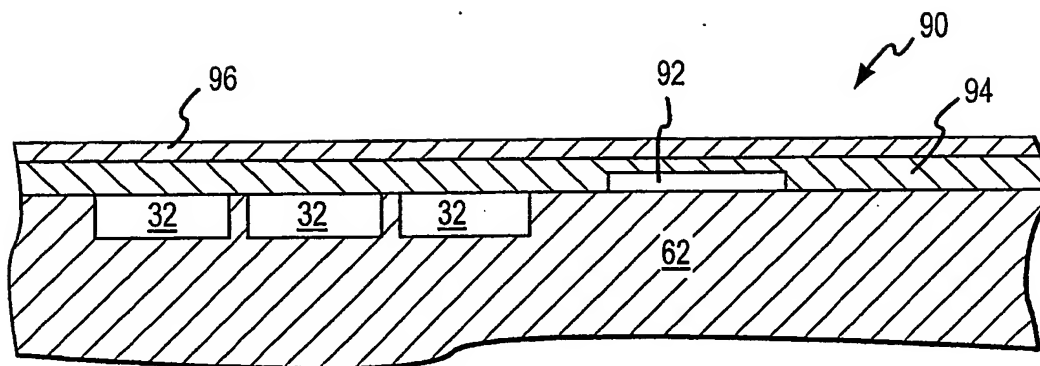


FIG.15

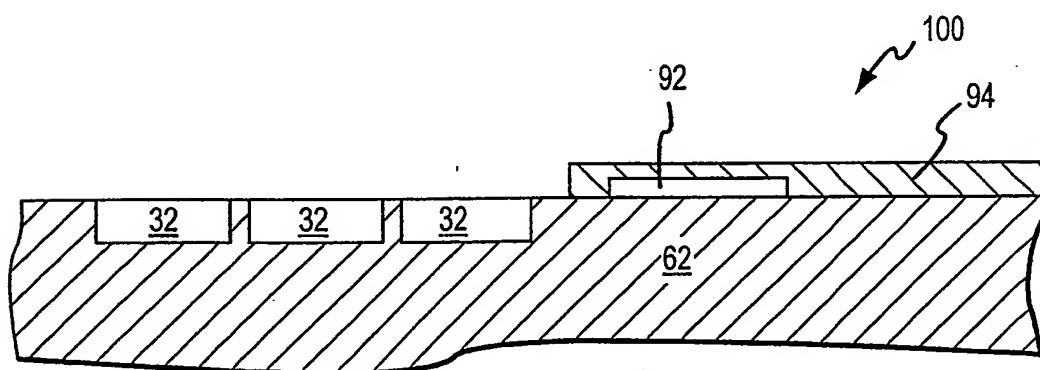


FIG.16

INTERNATIONAL SEARCH REPORT

PCT/IB 02/05193

A. CLASSIFICATION OF SUBJECT MATTER IPC 7 B06B1/06 G10K11/00 H01L41/08		
According to International Patent Classification (IPC) or to both national classification and IPC		
B. FIELDS SEARCHED Minimum documentation searched (classification system followed by classification symbols) IPC 7 B06B G10K H01L		
Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched		
Electronic data base consulted during the international search (name of data base and, where practical, search terms used)		
C. DOCUMENTS CONSIDERED TO BE RELEVANT		
Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 5 488 954 A (SLEVA MICHAEL Z ET AL) 6 February 1996 (1996-02-06) column 5, line 1 - column 6, line 19 column 7, line 11 - line 44 column 8, line 15 - line 17 abstract; figure 1 ---	1-7,9
X	US 5 406 163 A (CARSON PAUL L ET AL) 11 April 1995 (1995-04-11) column 4, line 62 - column 5, line 14 column 7, line 37 - column 8, line 29 column 9, line 39 - column 11, line 17 abstract; figures 1,4,6-8 ---	1-7,9
A	EP 0 404 154 A (TERUMO CORP) 27 December 1990 (1990-12-27) the whole document --- -/--	1-7,9
<input checked="" type="checkbox"/> Further documents are listed in the continuation of box C. <input checked="" type="checkbox"/> Patent family members are listed in annex.		
* Special categories of cited documents : "A" document defining the general state of the art which is not considered to be of particular relevance "E" earlier document but published on or after the international filing date "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified) "O" document referring to an oral disclosure, use, exhibition or other means "P" document published prior to the international filing date but later than the priority date claimed "T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention "X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone "Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art "Z" document member of the same patent family		
Date of the actual completion of the international search 10 March 2003		Date of mailing of the international search report 22.05.03
Name and mailing address of the ISA European Patent Office, P.B. 5818 Patentlaan 2 NL - 2280 HV Rijswijk Tel. (+31-70) 340-2040, Tx. 31 651 epo nl, Fax: (+31-70) 340-3018		Authorized officer Passier, M

INTERNATIONAL SEARCH REPORT

PCT/IB 02/05193

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT		
Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	US 5 956 292 A (BERNSTEIN JONATHAN J) 21 September 1999 (1999-09-21) abstract; figures 5,8,12 -----	1-7,9

INTERNATIONAL SEARCH REPORT

patent family members

PCT/IB 02/05193

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US 5488954 A	06-02-1996	NONE	
US 5406163 A	11-04-1995	US 5160870 A	03-11-1992
EP 0404154 A	27-12-1990	JP 3023849 A	31-01-1991
		JP 2919508 B	12-07-1999
		JP 3151948 A	28-06-1991
		AU 621757 B	19-03-1992
		AU 5765890 A	24-01-1991
		DE 69023555 D	21-12-1995
		DE 69023555 T	11-04-1996
		US 5212671 A	18-05-1993
US 5956292 A	21-09-1999	NONE	

Box I Observations where certain claims were found unsearchable (Continuation of item 1 of first sheet)

This International Search Report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1. ☐ Claims Nos.:
because they relate to subject matter not required to be searched by this Authority, namely:

2. ☐ Claims Nos.:
because they relate to parts of the International Application that do not comply with the prescribed requirements to such an extent that no meaningful International Search can be carried out, specifically:

3. ☐ Claims Nos.:
because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a).

Box II Observations where unity of invention is lacking (Continuation of item 2 of first sheet)

This International Searching Authority found multiple inventions in this International application, as follows:

1. ☐ As all required additional search fees were timely paid by the applicant, this International Search Report covers all searchable claims.

2. ☐ As all searchable claims could be searched without effort justifying an additional fee, this Authority did not invite payment of any additional fee.

3. ☐ As only some of the required additional search fees were timely paid by the applicant, this International Search Report covers only those claims for which fees were paid, specifically claims Nos.:

4. ☒ No required additional search fees were timely paid by the applicant. Consequently, this International Search Report is restricted to the invention first mentioned in the claims; it is covered by claims Nos.:

1-7, 9

Remark on Protest

- ☐ The additional search fees were accompanied by the applicant's protest.
- ☐ No protest accompanied the payment of additional search fees.

FURTHER INFORMATION CONTINUED FROM PCT/ISA/ 210

1. Claims: 1-7,9

Filled recess in substrate below transducer.

2. Claims: 8,10

Encapsulated transducer on reduced substrate.